

## Full length article

## Laser-assisted fabrication and in vitro verification of functionalized surface for cells biointegration

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## ARTICLE INFO

## Keywords:

Titanium implants  
Laser structuring  
Relief  
hMSCs  
Biocompatibility  
Osteogenic differentiation

## ABSTRACT

The paper investigates how the surface relief of an implant affects cell behavior. Currently, most implant manufacturers claim the key impact biocompatibility factor to be surface micro-roughness. We suppose that the interaction between cells and implants also depends on such relief peculiarities as continuous or discontinuous topography, subcellular distance between peaks and presence of porous oxide layer. We have developed the laser processing conditions that provide three different reliefs: «open grooves», «grid» and «close grooves». Along with the micro-roughness characteristics the reliefs differ with their deepness and period of grooves. The surface composition analysis results have shown a sandwich structure consisting of  $\text{Ti} \rightarrow \text{TiO} \rightarrow \text{Ti}_2\text{O}_3\text{Nx} \rightarrow \text{TiO}_2$  (anatase)  $\rightarrow \text{TiO}_2$  (rutile). The wettability study has demonstrated superhydrophilicity (CA is  $0^\circ$ ) for all reliefs. The quantitative and qualitative analysis of hMSCs proliferation and osteogenic differentiation was performed for 20 days. In vitro study has revealed the topography affects the spatial orientation of cells. The shape and size of the cell nuclei vary with different topographies. We have found continuous «open grooves» structures with the subcellular to cellular period are beneficial for cells' life-sustaining activity. Discontinuous «grid» structures with individual slots might not provide cells with mobility with the least external mechanical effect compared to «open grooves».

## 1. Introduction

The survival of dental implants is closely related to the long and painful period of postsurgical repair of surrounding tissues. Despite the relatively low failure rate of within 5% at 10 years or more of follow-upped implants [1], those who reject an implant have to restore lost bone tissue, fix a new implant and undergo a lengthy healing period, which may take from 3 to 6 months, following doctors' prescriptions. Thus, today the problem of implant survival remains relevant. The survival rate and long-term functioning of installed implants are affected by the quality of the implantation, oral hygiene during implant exploitation, as well as the characteristics of the implant itself, namely,

material, shape and structure of the surface [2]. Surgery process and oral hygiene depend on the dental surgeon's qualification and the patient's responsibility, respectively, but the surface characteristics enhancement is accessible to implant manufacturers. It was shown that surface relief, roughness, wettability and chemical composition of titanium implant surface are crucial points for its biocompatibility [3–9]. To change the relief and chemical composition, sandblasting methods, chemical etching and their combination [10–13], anodizing [14–18] and laser structuring [19–26] are the most frequently applied. Sandblasting allows to obtain a disordered developed relief by bombarding the surface with a powder jet directed under pressure. Usually, acid etching of the treated surface follows sandblasting to smooth some sharp peaks, but, as

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<https://doi.org/10.1016/j.optlastec.2020.106871>

Received 9 July 2020; Received in revised form 26 November 2020; Accepted 16 December 2020

Available online 12 January 2021

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a recent study showed,  $\text{Al}_2\text{O}_3$  particles still remain on the surface [27]. In the process of anodizing, by selecting the magnitude of electrical current and composition of an electrolyte, a porous relief with a pore size of  $\leq 8 \mu\text{m}$  is formed on the titanium surface [28,29]. Using the laser structuring with various processing modes and scanning patterns, it is possible to create a wide range of various reliefs: grooves [24,25,30–33], grids and craters [19,26,34], biomimetic microcones [35], nanoreliefs [36], etc. The width, depth, and period of laser-induced microstructures usually vary from units to hundreds of micrometers. Noteworthy, laser machining reduces surface contamination [37]. The formation of micro- and nanorelief in the process of anodizing and laser structuring is accompanied by various surface modifications of titanium oxide:  $\text{TiO}_2$  (rutile and anatase),  $\text{Ti}_2\text{O}_3$ ,  $\text{TiN}$ . The height of the oxide layer reaches from a few nanometers to several microns [28,29]. Titanium oxides increase the corrosion resistance of the implant [7].

The methods mentioned above are applied in the industrial production of dental implants. In this case the most commonly used parameters for surface characterization are usually a height-descriptive parameter average surface roughness ( $S_a$ ) (the arithmetic mean deviation of a surface) and hybrid parameter spell out ( $S_{dr}$ ) (the ratio between the area of the “real” developed surface and the area of the “projected” surface [38]). Roughness of different implant zones depends on implant manufacture:  $S_a$  from  $0.13 \mu\text{m}$  to  $1.49 \mu\text{m}$  and  $S_{dr}$  from 1.7% to 172.7% (Nobel Biocare AB, Göteborg, Sweden) [28];  $S_a$  from  $1.78 \mu\text{m}$  to  $2.1 \mu\text{m}$  (Institut Straumann AG, Basel, Switzerland) [39,40];  $S_a$  from  $1.1 \mu\text{m}$  (Astra Tech Dental AB, Mölndal, Sweden) [34];  $S_a$  from  $0.3 \mu\text{m}$  to  $0.68 \mu\text{m}$  (Biomet, Palm Beach Gardens FL, USA) [41]. According to the review [42] the authors conclude the “optimal” range is from  $1 \mu\text{m}$  to  $2 \mu\text{m}$ , based on the studies where  $S_a$  range from  $0.6$  to  $11.0 \mu\text{m}$  was analyzed. On the other hand, very rough surfaces may leave such a distance between peaks that cells perceive them as smooth surfaces. However, there are works in which  $S_a$  surface about  $9 \mu\text{m}$  indicates high biocompatibility for bone regeneration of titanium implants [43]. As was shown by computerized simulation in [44], the lateral resolution of an instrument/method of surface roughness estimation significantly limits measurements’ accuracy.

We hypothesized that roughness  $S_a$  significantly exceeding  $2 \mu\text{m}$  can also give a positive bone response if the distance between peaks is considered. The research for the neural stem cells (NSCs) demonstrated that the type of topography, continuous or discontinuous, the size of single elements of relief and their relative position affect the spatial orientation of NSCs [45,46]. It was also shown that alternating grooves (continuous topography) with subcellular and cellular width strongly promote neurite guidance and orientation along the grooves. Discontinuous topographies with subcellular to cellular scales influence different lineage differentiation.

However, the question remains, whether the cells-implants interaction between cells and implant surfaces is affected not only by surface micro-roughness (parameters  $R_a$  /  $S_a$ ,  $S_{dr}$ , etc.), as most implant manufacturers claim, but also by the relief, which includes continuous or discontinuous topography, the subcellular distance between peaks (or period of the microstructure) and the presence of nanoparticles. We suppose such a complex surface structure is justified for several reasons. To fix cells to the surface, they need a relatively rigid but hydrophilic base. For a long-life span and reproduction (proliferation) on the surface, they need oxygen for breathing, heat and ventilation for removing waste products, as well as conditions for sleep and rest - suppleness (softness) of a substrate and its ventilation. To remove waste products, hydrophobic channels are necessary. Today, a comprehensive study that considers both the technological aspects of creating such a surface for titanium implants and preclinical study of their effectiveness is required. This work aims to verify the hypothesis which states that bone cells need not only a rough surface for fixing but also a special relief to provide the comfortable life-sustaining activity of cells throughout their lives.

We have conducted an in vitro study for human bone marrow mesenchymal stem cells (hMSCs). By laser processing, we developed

three different reliefs with the subcellular and cellular period of microstructures (tens of microns) that enable certain mobility of cells along with the least external mechanical affect. Two types of continuous reliefs, «open grooves» OG and «close grooves» CG, and discontinuous relief, «grid» G, were fabricated on 6Al4V-titanium surface. To increase cell - surface connection area, groove and grid sidewalls were made rough. We have investigated the cellular activity on these reliefs and compared them with each other and with an untreated smooth surface.

## 2. Material and methods

### 2.1. Surface relief engineering and investigation

Titanium alloy Ti–6Al–4V discs (1 mm thickness, 5 mm diameter) and flat plates (with dimensions  $5 \times 5 \text{ cm}$ ) were filed down with 100–2000 grid sandpapers and polished to the mirror-like surface ( $R_a = 0.6 \pm 0.02 \mu\text{m}$ , measured on profilometer Hommel Tester T8000) with diamond paste ( $R_a = 0.5 \mu\text{m}$  and  $0.1 \mu\text{m}$ ) using a Dremel mini drill. Samples were cleaned from contaminations in an ultrasonic bath filled with distilled water, acetone and isopropanol consequently. After that, the samples were stored under normal ambient air conditions.

Fabrication procedures. The surface of the titanium alloy disks was processed by the ytterbium pulsed fiber laser. The laser wavelength was  $1064 \text{ nm}$ , the average laser power was  $1\text{--}20 \text{ W}$ , the pulse duration was  $100 \text{ ns}$ , and the repetition rate was  $10\text{--}100 \text{ kHz}$ . In our experiments, laser radiation was focused in the spot of  $50 \mu\text{m}$ , the focal length is  $184 \text{ mm}$ ,  $M^2$  is  $1.99$ . No assist gas was used during the experiments to control the degree of oxidation during the processing. Laser processing was performed in the air under normal conditions. Line-by-line scanning of the disk surface was performed with overlapping laser pulses along the X-axis with the step of  $M_x$  and the Y-axis with the step of  $M_y$  (Fig. 1).

Laser processing conditions of all reliefs are summarized in Table 1, where  $P$  – average power,  $f$  – pulse repetition frequency,  $v$  – scanning speed,  $N$  – number of loops,  $I$  – intensity (calculated as the ratio of the peak power to the cross-sectional area of the laser beam waist),  $M_x$  – X-axis overlapping,  $M_y$  – Y-axis overlapping. These laser processing conditions provide heating the titanium surface above the evaporation threshold.

CG relief is formed under laser exposure modes below the evaporation threshold, on the other hand, G and OG reliefs are formed above the evaporation threshold. During the first pass of laser radiation on the surface of all samples (when it is heated above the melting point), a molten pool is formed and under the pressure of recoil vapors the material is ejected with the formation of rolls along the edges. Heating the metal above the evaporation threshold (for G and OG reliefs) promotes more intense evaporation and increase in groove depth. So, we form massive grooves by removing current groove relative to the previous one on value  $M_y$ .

To form the G and CG reliefs, the second pass of laser radiation is

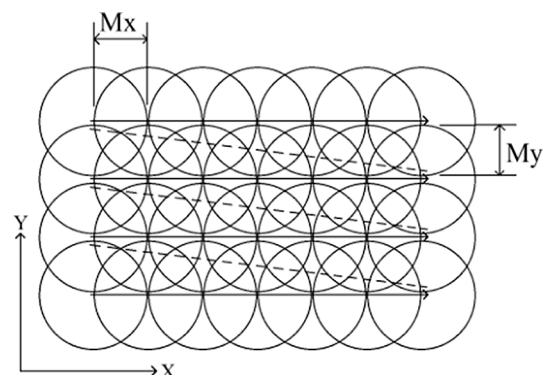


Fig. 1. Overlapping of laser pulses along the x-axis  $M_x$  and along the y-axis  $M_y$ .

**Table 1**

Laser processing conditions for the «open grooves» OG, «grid» G and «close grooves» CG reliefs.

Relief	P, W	f, kHz	v, mm/s	N, line/mm	I, W/cm <sup>2</sup>	Mx, μm	My, μm
OG	3.00	1.6	5	11	$5.7 \cdot 10^7$	3	90
G	8.18	60	200	20	$5.7 \cdot 10^7$	3	40
CG	2.65	20	15	30	$2.7 \cdot 10^7$	3	40

carried out in the orthogonal direction in relation to the first pass with the same laser parameters.

For CG relief formation the grooves from the first pass almost remelt (without deep channel formation). After the second pass (in the orthogonal direction) the narrow grooves are obtained by repeated laser exposure. When the second pass of G relief formation, the same grooves are formed in the orthogonal direction. Deep slots are formed at the center's intersection of two orthogonal grooves.

To form OG relief, the second and the third passes of laser radiation is carried out in the parallel direction with a step of My value relative to the previous pass.

The diagrams of scanning patterns for G, CG and OG reliefs are presented in Fig. 2.

A total of 36 disk-shaped samples and 12 flat square plates with laser-induced structures were fabricated. To test the repeatability of the structures 5 random samples for every structure were selected, then the standard deviation (3–6 μm) was calculated.

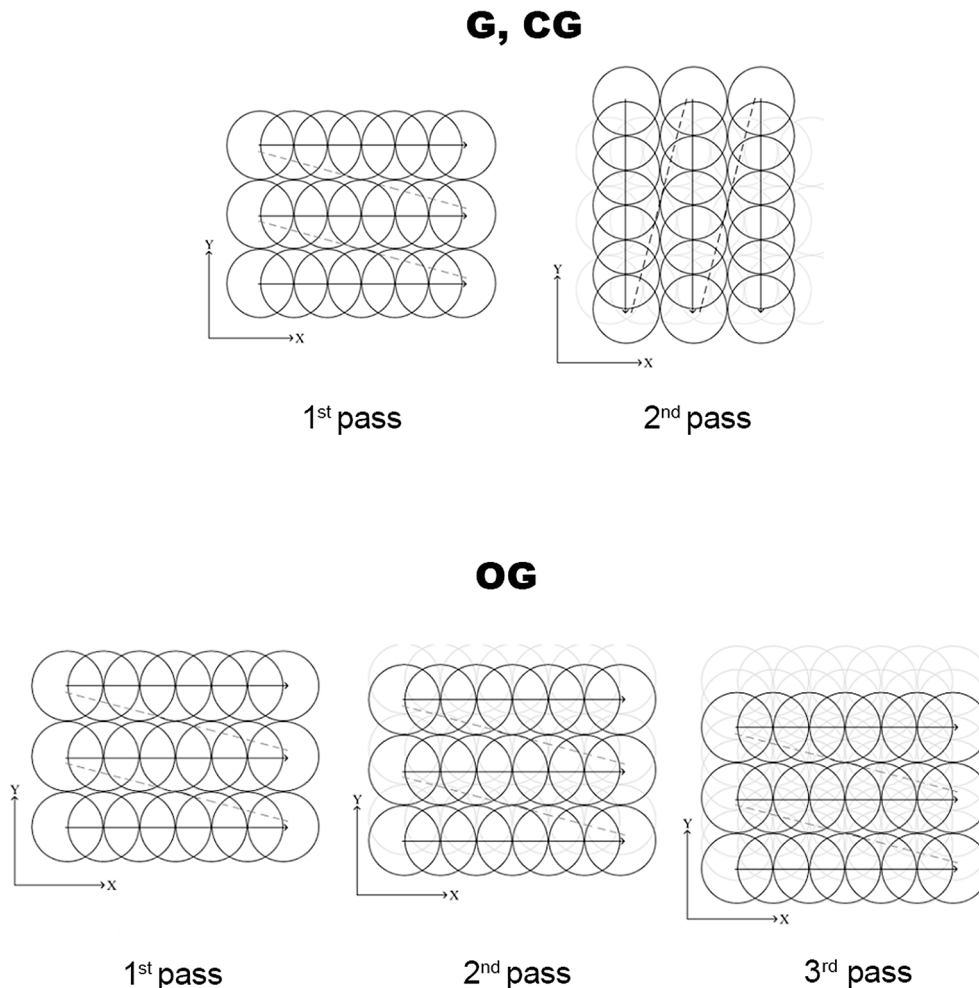
Surface topographic analysis. Roughness measurements were

performed on contact profilometer Hommel Tester T8000. The measurement area was  $300 \times 300 \mu\text{m}$ . The resolution of the instrument is 100 nm, the accuracy, according to DIN 4772 is Class 1. Measurement error is  $\pm 1 \mu\text{m}$ . Surface roughness parameters such as Sa and Sdr were calculated. All areas were measured 3 times for each experimental sample to evaluate their stability and calculate standard deviation of the data.

**Surface wettability.** The measurements of the static contact angle (CA) were performed with a home-developed setup based on the LED arrangement source (summary power 1 W) and high-resolution CCD camera TouPCam. The setup does not enable the measurement of the dynamic contact angles. Distilled water was used as a test liquid. An CCD camera was used with a sample rotation stage enabling 360° contact angle measurements of the deposited droplet. A minimum of three droplets was analyzed in each condition to determine the contact angle values. The volume of the droplet was 0.5 μl. The CA was measured immediately following the laser treatment. The Digimizer software was used to measure the CA. Aging effect was not studied.

**Scanning electron microscopy (SEM) analysis** was performed using microscopes FEI Helios 660 (at electron and ion modes) and FEI Quanta 600 with field emission, equipped with an energy dispersive spectrometer (EDX) (EDX-analysis resolution is 0.20–0.25%, elements from Be).

A field-enhanced emission microscope Tecnai G2 F20 equipped with an EDAX system for x-ray microanalysis with a silicon drift detector was used to study nanosecond laser treatment's effect on the phase structural state of the near-surface layers of titanium alloy. The preparation of thin cross-section foils for TEM was conducted using focused ion beam (FIB)



**Fig. 2.** Scanning patterns of G, CG and OG reliefs.

of scanning electron-ion microscope FEI Helios 660. Platinum was used as a protective material for a region of interest and deposited using gas injector systems (GISs) integrated into a microscope camera. The sample with a thickness of about 100 nm and a region of interest of about  $7.5 \times 7.5 \mu\text{m}^2$  was prepared by gradual ion thinning and used for subsequent transmission electron microscopy (TEM) analysis.

## 2.2. In vitro analysis

We used human bone marrow mesenchymal stem cells (hMSCs) that were isolated from bone marrow of normal donors with their informed consent according to the institutional guidelines under the approved protocol described elsewhere [47]. The hMSCs were isolated and characterized by flow cytometry (Cell Lab Quanta SC, Beckman Coulter, USA) as described previously [47]. The common markers to human MSCs (CD34, CD45, HLA-DR, CD105, CD44, CD54, CD73, and CD90) were studied. The cells (indicated hMSCs-TurboFP635) were stably transfected with a gene of far-red fluorescent protein TurboFP635 (lentiviral transfer vector LVT-TurboFP635, Evrogen, Russia) according to the protocol also described in [47]. The cells were cultured in MesenCult™ MSC Basal Medium supplemented with MesenCult™ MSC Stimulatory Supplement (Stemcell Technologies, Canada) and 0.58 mg/ml L-glutamine (PanEco). The cell culture was maintained at 310 K in a 5% CO<sub>2</sub> humidified atmosphere.

Titanium samples were placed on a 48-well plate, sterilized under UV light for 30 min and individually seeded ( $5 \cdot 10^4$  hMSCs-TurboFP635 per implant) with cells in the third passage. The cells were seeded on the samples with laser-modified surface in the same day as the ones were fabricated. The fluorescence of the hMSCs-TurboFP635 was detected using a Leica DM IL LED Fluo microscope equipped with TX2 filter cube (Germany). Fluorescence imaging was performed on days 1, 5, 10, 15 and 20 after cell seeding. To estimate the number of cells on the implants, we used a unique technique developed earlier for bone scaffolds and labeled cells. The details of the processing methodology can be found in [47].

On day 20 we analyzed the osteogenic differentiation of the seeded cells. We assessed osteocalcin expression in the cells and alkaline phosphatase (ALP) activity in a culture medium. Osteocalcin is the most abundant noncollagenous bone protein that constitutes 1–2% of the total matrix proteins. Osteocalcin is exclusively secreted by osteoblasts and recognized as an early marker of in vitro osteogenic differentiation of mesenchymal stem cells [48]. ALP is one of the most commonly used markers of mesenchymal stem cells' osteogenic differentiation in vitro. This metalloenzyme is an important component in hard tissue formation, highly expressed in mineralized tissue cells [49].

We performed immunocytochemical staining with the anti-osteocalcin antibodies (Anti-Osteocalcin Picoband™ Antibody, Boster Biological Technology, USA). The immune complex was visualized using Opal 520 TSA Plus (Opal kit, Perkin-Elmer, Waltham, MA). The cell nuclei were stained with Hoechst 33,342 (Thermo Fisher Scientific, USA). The Opal 520 fluorescence signal was detected using a Leica DM IL LED Fluo microscope equipped with I3 filter cube. The Hoechst 33,342 was observed using an A4 filter cube (Germany).

To assess ALP activity, we conducted a fluorometric assay of culture medium harvested from the implants with cells (Alkaline Phosphatase Detection Kit, Fluorescence, Sigma, USA). The fluorometer (Synergy™ Mx Multi-Mode Microplate Reader, BioTek Instruments, Inc., USA) was set to 360 nm excitation and 440 nm emission. A medium with no secreted ALP was served as a negative control, which indicated the background level.

All staining procedures were done according to the standard protocols of Sigma, Thermo Fisher Scientific, Boster Biological Technology, Perkin-Elmer.

All in vitro experiments and experimental protocols were approved by the Research Ethics Board of the Nizhny Novgorod State Medical Academy (Privolzhsky Research Medical University, Nizhny Novgorod,

Russia) and obtained according to the principles of the Declaration of Helsinki.

## 3. Results and discussion

### 3.1. Surface relief and wettability

We have studied three different reliefs on the titanium surface by pulsed fiber laser: «open grooves» OG, «grid» G and «close grooves» CG. The choice of these three surface structures is based on the two-stage classification [46], including continuous and discontinuous topographies. In current investigation, we have developed laser processing conditions that provide the formation of well-ordered reliefs (Fig. 3) which consist of a microrelief on the walls of grooves and slots (Fig. 3B) to fix cells on the surface better and a porous oxide layer (Fig. 3C) for protein adhesion in the early stages of biointegration. The nanotopography on the surface of the reliefs is unintentionally produced. These features appear due to non-controllable processes - inverse precipitation of evaporated material from the surface that occurs during the laser treatment [50].

Using scanning electron microscopy, the structures' period was calculated. The period of the OG relief is  $30.2 \pm 2.4 \mu\text{m}$ . The period of the G relief is  $49.5 \pm 4.6 \mu\text{m}$ . The period of the CG relief is  $31.4 \pm 3.3 \mu\text{m}$ .

Using contact profilometry height-descriptive Sa and hybrid Sdr parameters of untextured titanium and the reliefs surface were measured (Table 2). The roughness of Ti reference sample is 0.42  $\mu\text{m}$  (Sa) and 6.65% (Sdr). The roughness of «open grooves» is 3.85  $\mu\text{m}$  (Sa) and 46.57% (Sdr). The roughness of «grid» 11.81  $\mu\text{m}$  (Sa) and 272% (Sdr). The roughness of «close grooves» is 3.26  $\mu\text{m}$  and 43.08% (Sdr).

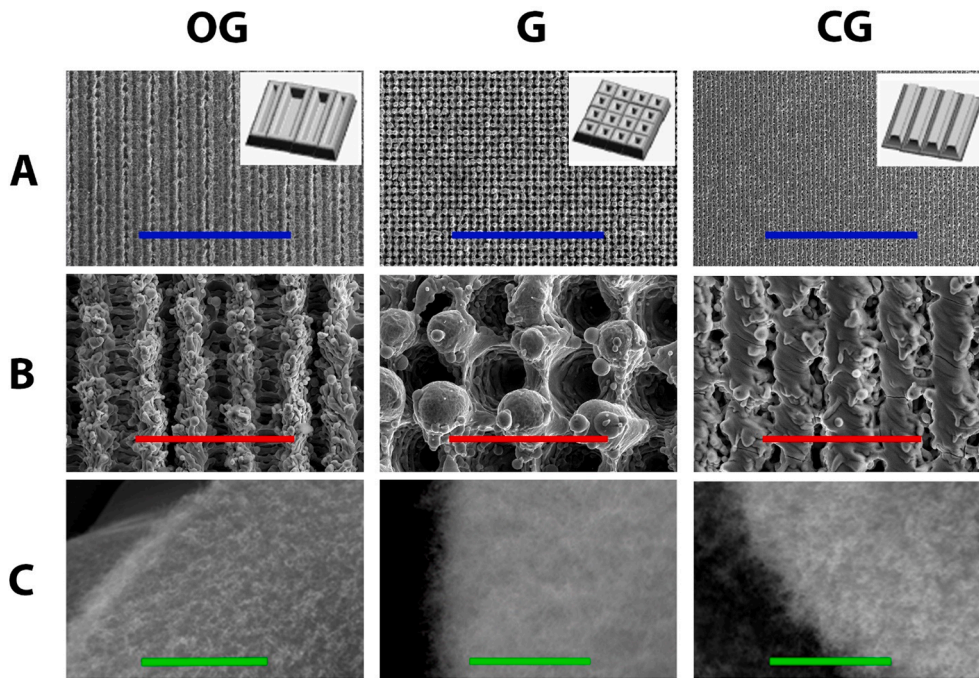
We obtained 3D surfaces (Fig. 4) of the samples' reliefs cross-sections (Fig. 4).

The initial surface of our samples was hydrophilic (contact angle is  $(70 \pm 1)^\circ$  (Fig. 5A). We have revealed that measuring CA of the structured samples is impossible. A drop instantly spreads over and penetrates the surface. Fig. 5B demonstrates the area change of spreading a drop over time as a percentage, where  $35 \times 35 \text{ mm}$  square area is 100%. Moreover, the direction and maximum spreading area are different for all the samples. The top view screenshots demonstrate the trace of the drop at the moment when it stops spreading (Fig. 5B): CG – 10 s; G – 17 s, OG – 24 s. Spreading area of a droplet on Ti reference sample is constant in time. The maximum spreading area is on OG relief. As seen, the fluid extends along the grooves.

Therefore, initiated specific laser parameters have led to changing the surface wettability from hydrophilic to superhydrophilic. It is worth noting that the superhydrophilic surface demonstrates far more highly developed proliferation against superhydrophobic surface. On the one hand, the protein adsorption amount on the hydrophilic surface is significantly more significant than that on the hydrophobic surface [51]. The protein adsorption behavior also plays an important role in cell adhesion. On the other hand, the work [52] casts doubt on the fact that protein adsorption and cell proliferation occur on any hydrophilicity surface, i.e., the factors providing high wettability and the factors providing protein adsorption and cell proliferation are not equivalent. Therefore, additional experiments are required to identify which factor has a strong influence on cell adhesion. However, it should be noted that in our case, one of the factors affecting superhydrophilicity properties is high oxygen content. So, a high oxygen content leads to an increase in protein adsorption, which was also discussed in [52].

EDX-analysis of the surface chemistry showed a significant oxide increase for the laser-treated titanium (Table 3) compared to the non-treated titanium. The oxide percentage for the surface of OG, G and CG reliefs varies within a ratio from 27.42 to 32.73 wt%. Then we accepted that the relief formatting was conducted under similar conditions, so their chemical composition is analogous. We study the effect of nanosecond laser treatment on the phase composition of the near-surface layers only for OG relief.





**Fig. 3.** SEM images of the «open grooves» OG, «grid» G and «close grooves» CG reliefs on microscale (A, B) and nanoscale (C). The scale bars are: 1 mm (blue), 100  $\mu\text{m}$  (red) and 1  $\mu\text{m}$  (green).

**Table 2**

Roughness of the Ti-surface before (Ti reference) and after (OG, G, CG) laser treatment.

Sample	Sa, $\mu\text{m}$	Sdr, %
Ti reference	$0.42 \pm 0.004$	$6.65 \pm 0.09$
Open grooves OG	$3.85 \pm 0.060$	$46.57 \pm 5.20$
Grid G	$11.81 \pm 0.150$	$272.00 \pm 22.30$
Close grooves CG	$3.26 \pm 0.010$	$43.08 \pm 2.30$

Using the focused ion beam method in the SEM column, the thin cross-section foil was cut (sample with OG relief) to determine its chemical composition. As a result of ion thinning, a sample with a surface area of  $7.5 \times 7.5 \mu\text{m}^2$ , with a thickness of approximately 100 nm, was obtained for subsequent investigation by TEM (Fig. 6A).

Study of the cross-section foil demonstrated that its structure is a branched system of sub-micrometer, micrometer and nanostructures (Fig. 6B). Four zones can be indicated that differ in morphology and phase contrast. Identifying microdiffraction and Fourier transform obtained from images with atomic resolution showed that layers vary in phase composition:  $\text{TiO}$ ,  $\text{Ti}_2\text{O}_3$  and  $\text{TiO}_2$  (in the phase of anatase) from depth to surface (Fig. 6, top row). According to the electron-microscopic analysis, the surface layer consists mostly of the agglomerates of  $\text{TiO}_2$  (in the phase of rutile nanoscale particles with size about 5 nm). The formation of a columnar morphology and the oxide layer's porosity is due to the deposition of the oxidized products on the substrate (modified titanium alloy surface), related to laser ablation. The values of experimental interplanar distances compared to the reference data are shown in Table 4.

A thin layer of about 70 nm can be seen between  $\text{TiO}$  and  $\text{Ti}_2\text{O}_3$  layers (at high magnifications). This layer consists of two layers (Fig. 6C). According to EDX analysis in TEM, the nearest to the surface layer is rich with oxygen, and the layer under it contains nitrogen. EDX data in local areas with a diameter of about 2 nm (local analysis in TEM) as well as the data of element analysis along the line (depth profile) correlate with electron-microscopic analysis data. With an increase in depth, the concentration of oxygen decreases. The data given suggests

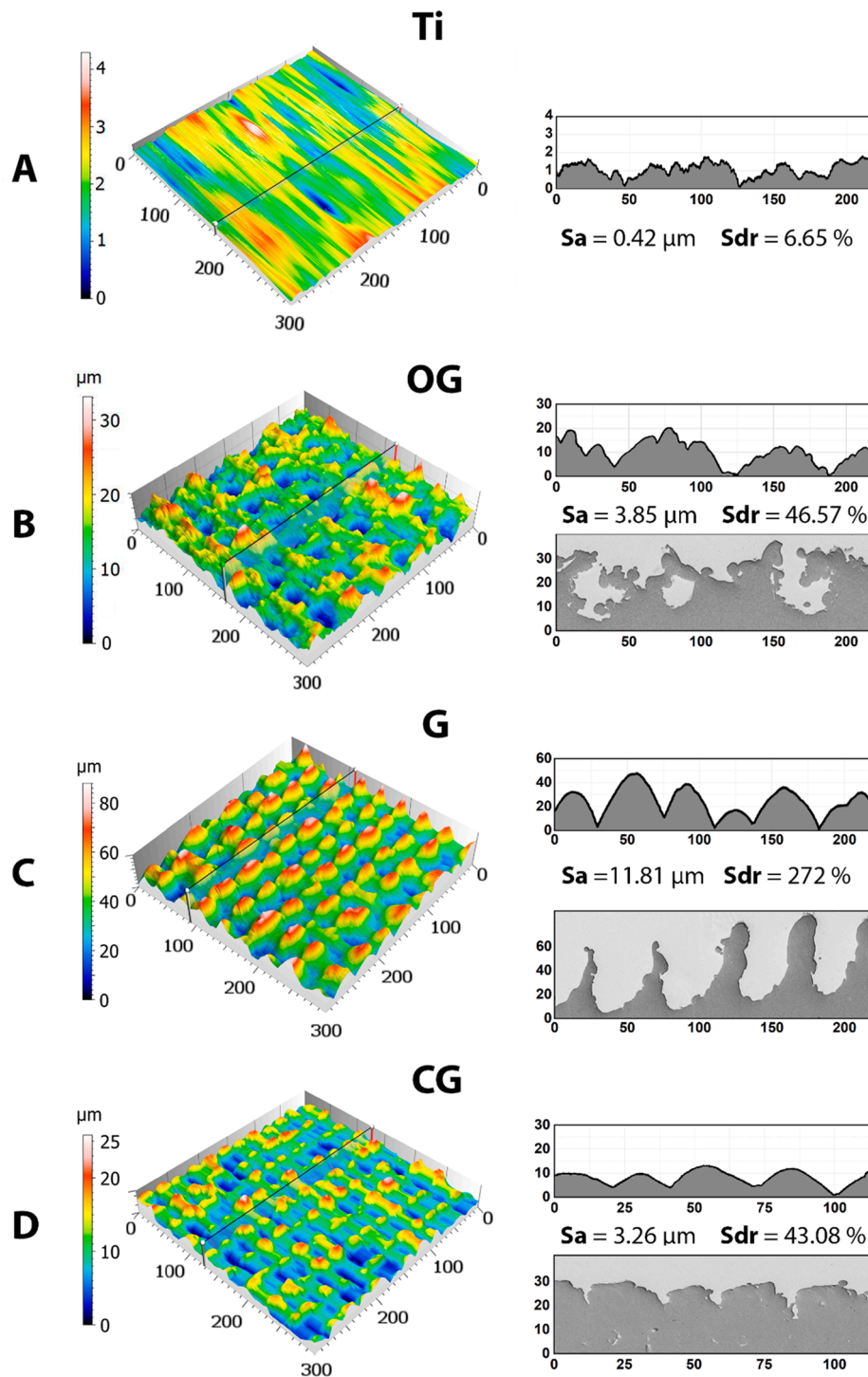
the phase transition with a formation of layered oxide structures of various phase composition occurring on the modified surface, which correlates with theoretical calculations [55].  $\text{Ti}_2\text{O}_3$  crystallites are rich with nitrogen, and  $\text{Ti}_2\text{O}_3\text{N}_x$  phase with distorted hexagonal lattice is present because nitrogen (interstitial impurity) fits into lattice interstices. Calculations showed that parameter "a" of the lattice increases, whereas parameter "c" decreases (Table 4).

The titanium oxynitride coatings have high values of nanohardness and Young's modulus [55,56], but have no direct effect on cell behavior. Nevertheless, our nanostructures consist of these oxides. As was shown in [57,58], a nanorelief enhanced interaction with cells and biological fluids at the early stages of biointegration.

### 3.2. Analysis of cell proliferation, depthward colonization and osteogenic differentiation

For in vitro investigation we used hMSCs, that are a good model environment for studies at the early stages of osseointegration. A series of in vitro tests were conducted on the reliefs obtained compared to the original polished titanium alloy (Ti). The dynamic colonisation and hMSCs-Turbo FP635 cells proliferation was comparatively studied over 20 days using fluorescent imaging (Fig. 7). Quantitative analysis of cell proliferation on the implant's surface via fluorescent bioimaging of hMSCs-Turbo FP635 is presented in Fig. 8.

After 24 h, the seeded cells were found on all types of samples. On Ti the cells were arranged in an even layer and had a fibroblast-like elongated shape indicating their normal adhesion. Day after day the number of viable cells decreased from the initial quantity and reached zero point on day 20. After the first 24 h G and CG reliefs had single round-shaped hMSCs-TurboFP635, characteristic of incomplete adhesion to the surface. On day 20 the number of viable cells reached 165 650 cells/sample for CG and 196 000 cells/sample for G, respectively. On OG relief the cells were arranged in an even layer and had a fibroblast-like elongated shape indicating their normal adhesion on the first day after seeding. Fig. 6 demonstrates the most considerable proliferation for each day of investigation. The final value reached 266 500 cells/sample - the maximal number among all samples.

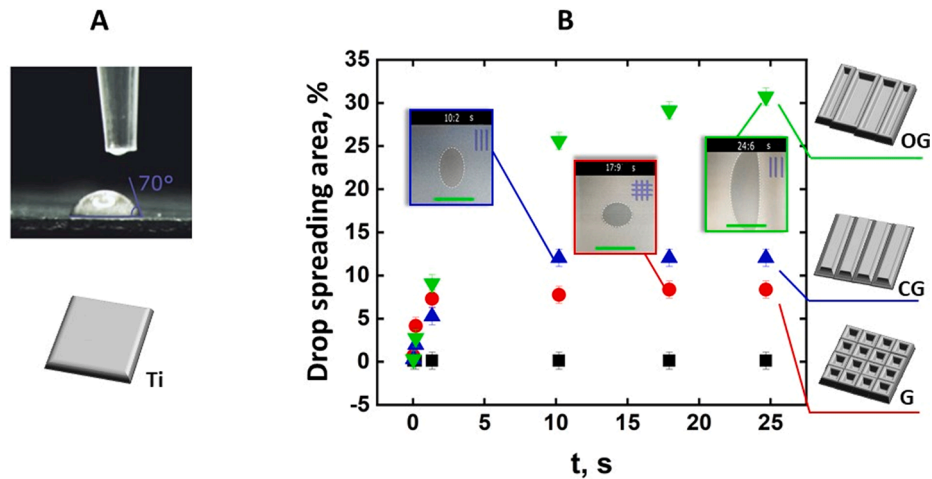


**Fig. 4.** 3D surfaces of the reliefs; calculated three-dimensional parameters Sa and Sdr; profiles and cross-sections of the «open grooves» OG (A), «grid» G (B) and «close grooves» CG (C).

The analysis of cell alignment indicates that OG and CG reliefs have an impact on directed cells growth. Interestingly, the cells elongated in the grooves were found on the first day for OG relief and day 10 for the CG relief.

It should be noted that the quantitative analysis does not take into account the cells that germinate inwards into the open pores. Qualitative analysis of cell growth into the implant from the surface on day 20 is demonstrated in Fig. 9. The results obtained show that the cells are located not only on the tops of the topographies but also cover their bottom and grow inward in open pores.

Osteogenesis was investigated through an expression of osteocalcin and an ALP activity test. Qualitative analysis of osteocalcin expression via immunocytochemical staining of the hMSCs with the anti-osteocalcin antibodies on day 20 is shown in Fig. 10. Osteocalcin is the most informative marker of bone formation. Osteocalcin is released by osteoblasts during osteogenesis. Green fluorescence indicates osteocalcin (Opal-520 staining), blue fluorescence - cell nuclei (Hoechst 33,342 staining). All reliefs develop some quantity of osteocalcin. The minimum of osteocalcin corresponds to CG relief. G and OG reliefs have approximately the same quantity of osteocalcin.



**Fig. 5.** The CA measurements of the unstructured titanium surface side elevation (A). The area change of spreading of a drop over time as a percentage out of  $35 \times 35$  mm square area (B) for the «open grooves» OG, «grid» G and «close grooves» CG reliefs, top view screenshots show the trace of the drop at the moment when it stopped spreading. The scale bar is 2 cm (green).

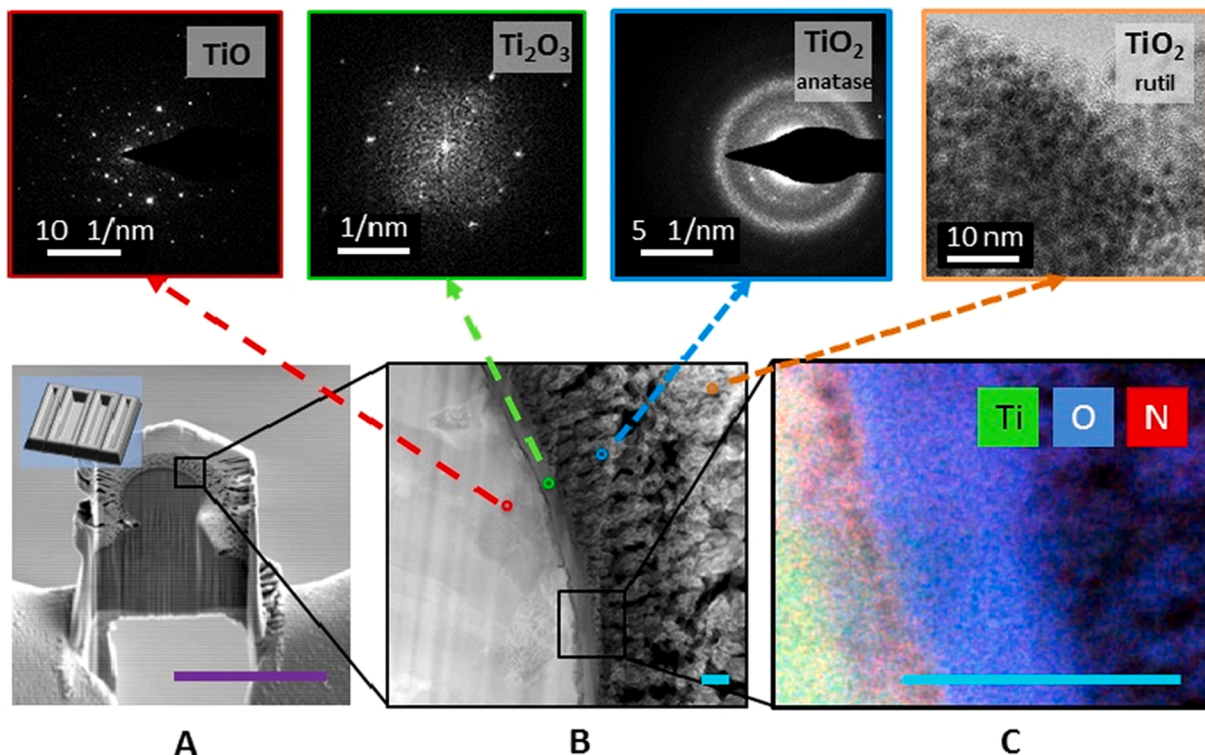
**Table 3**

Elemental composition of the Ti-surface before (Ti reference) and after (OG, G, CG) laser treatment (EDX-analysis).

Element, wt %	Ti	Al	V	O
Ti reference	89.41	5.56	4.82	0.21
OG	66.04	3.07	3.47	27.42
G	61.10	2.66	3.51	32.73
CG	62.02	4.52	3.44	30.02

The fluorescence imaging shows the differences between shapes and sizes of the cell nucleus for each sample. The nuclei of the cells cultured on G and CG reliefs have a rounded shape and the same size. For OG relief the cell nucleus is oval-shaped and possesses the smallest size compared to the other reliefs.

The second osteogenesis marker was the ALP activity (Fig. 11). The background level - a medium with no secreted ALP, served as a negative control. ALP was determined in all reliefs. The results correlate with the expression of osteocalcin results. Maximum ALP activity is observed for OG relief, a minimum - for CG relief. ALP activity of the G relief is similar to that one of the CG relief in view error.



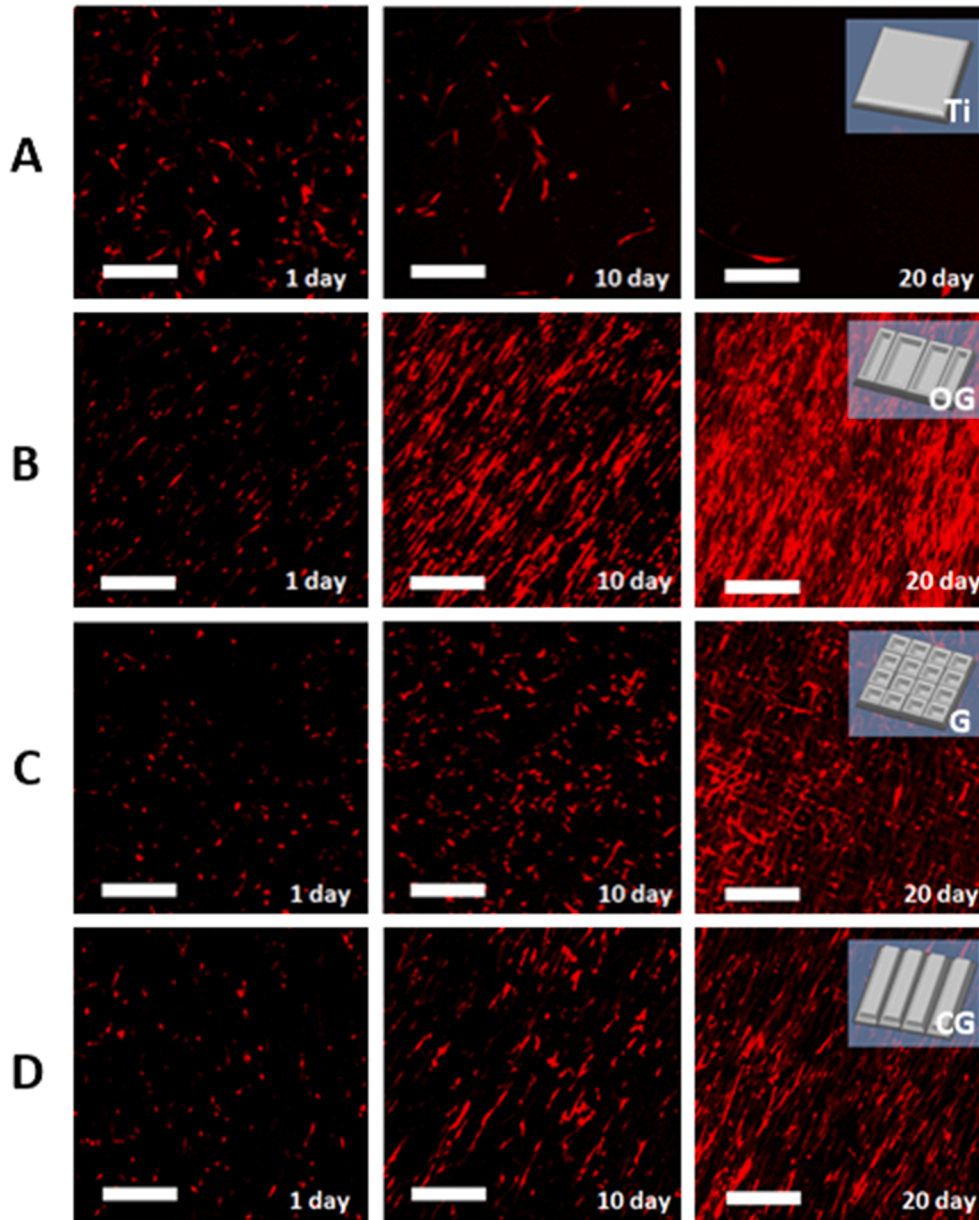
**Fig. 6.** SEM and TEM-images of titanium alloy sample after laser structuring for the «open grooves» OG sample. Bottom figures: (A) SEM-image of cross-section of a sample cut out with an ion beam for the following FIB thinning; (B) general cross-section view after FIB thinning; the dark-field contrast in STEM mode; top figures: an image of a transition layer with microdiffraction and Fourier transform; (C) Ti, O, and N - distribution maps of the cross-section. EDX in TEM. The light-field contrast in STEM. Color dots identify the qualifying distribution of the Ti-oxide phases. The scale bars are 20  $\mu\text{m}$  (violet), 100 nm (blue).



**Table 4**

Values of interplanar distances of titanium oxide phases (experimental and reference).

TiO <sub>2</sub> (rutile)		TiO <sub>2</sub> (anatase)		TiO		Ti <sub>2</sub> O <sub>3</sub>		Ti <sub>2</sub> O <sub>3</sub> with N
tetragonal lattice [53], a = 2.959 Å; b = 4.593 Å c = 4.593 Å	exp. meas.	tetragonal lattice [53], a = 3.784 Å; b = 3.784 Å c = 5.458 Å	exp. meas.	cubic lattice [54], a = 2.95 Å	exp. meas.	hexagonal lattice [55], a = 5.146 Å; c = 13.547 Å	exp. meas.	exp. meas., hexagonal lattice [56], a = 5.2 Å; c = 13.235 Å
3.248 (110)	3.21	3.516 (101)	3.60	2.412 (111)	2.50	3.723 (012)	3.74	3.52
2.488 (101)	2.48	2.431 (103)	2.44	2.089 (200)	2.20	2.696 (104)	2.70	2.67
2.297 (200)	2.30	2.379 (004)	2.38	1.477 (220)	1.40	2.573 (110)	2.6	2.55
2.187 (111)	2.20	1.758 (202)	1.76	1.259 (311)	1.26	2.235 (11-3)	2.22	–



**Fig. 7.** Typical fluorescent micrographs of the seeded hMSCs Turbo FP635 for 20 days (1st – 10th – 20th day). Ti-reference (A), OG (B), G (C), CG (D) reliefs. The cells are shown in red according to the fluorescence of TurboFP635. The number of cells is shown only on the top of the structures (it should be noted that the surface area is different for 4 samples). The scale bars are 300  $\mu\text{m}$  for all images.

In general, osteogenic differentiation requires sufficient attachment of multipotent MSCs to the substrate (implant) and their subsequent spreading [59,60]. Cells attach to the substrate by a focal contact (focal adhesions) [61,62]. The main molecules of focal contacts are integrins, which consist of the  $\alpha$ - and  $\beta$ -subunits [63]. They ensure the attachment

of cells to the substrate. Integrins are sensitive to the biochemical and biophysical characteristics of cellular substrates. Thus, osteogenic cells, using integrin receptors [63], assess the quality of the substrate: the rigidity of the substrates, their chemical composition, and surface topography.



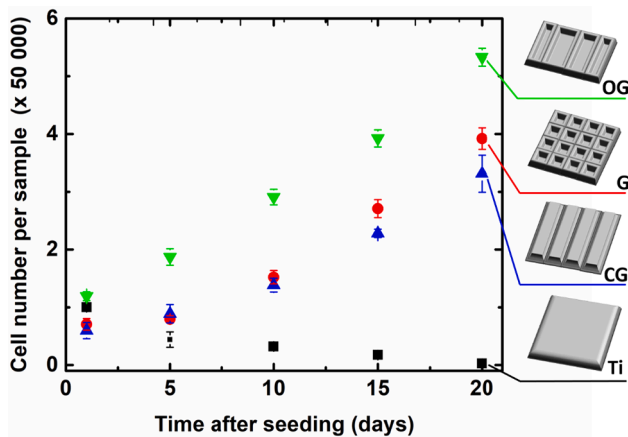


Fig. 8. Quantitative (1st – 5th – 10th – 15th – 20th days) analysis of cell proliferation for 20 days for the OG, G, CG and Ti reference surface.

In our case, if the chemical composition played a decisive role in osteogenic differentiation of MSCs, the percentage increase of oxygen on the sample surface would occur in accord with increase of ALP activity in the following order: CG, G, OG. However, this is not so: the maximum amount of oxygen corresponds to the OG relief, the minimum - to the G relief. The same can be said about the rigidity of the surface because it

directly depends on the chemical composition and crystal structure of the surface, although such an assessment has not been carried out. Thus, the difference in osteogenic differentiation for various surface reliefs is associated precisely with its geometric structure. From this point of view, grooves with a width and depth commensurate with the cells size make it possible for cells to spread in both directions. It is possible, a larger number of focal contacts for the OG sample is formed due to the presence of the most developed relief on the groove walls in comparison with the G and CG reliefs. Thus, the microrelief plays a decisive role in the firm adhesion of cells to the surface. It should be added that for deep analysis of reasons why various surface reliefs induced different osteogenic differentiation, it is necessary to study the mechanisms of attachment and spreading of single MSCs on reliefs, which is our future research topic. Nevertheless, observed cells behavior is related to the chemical composition change together with the relief change.

#### 4. Conclusions

In the present work, we have used the nanosecond laser structuring for changing the chemical composition and surface relief for Ti-6Al-4V titanium disks of 1 mm thickness and 5 mm diameter. We have developed the laser processing conditions that provide the formation of well-ordered rough surface with subcellular to cellular period of structures. The following reliefs have been formed: «open grooves» with the period of  $30.20 (\pm 2.40) \mu\text{m}$ ,  $S_a = 3.85 (\pm 0.06) \mu\text{m}$  and  $S_{dr} = 46.57 (\pm 5.20) \%$ ;

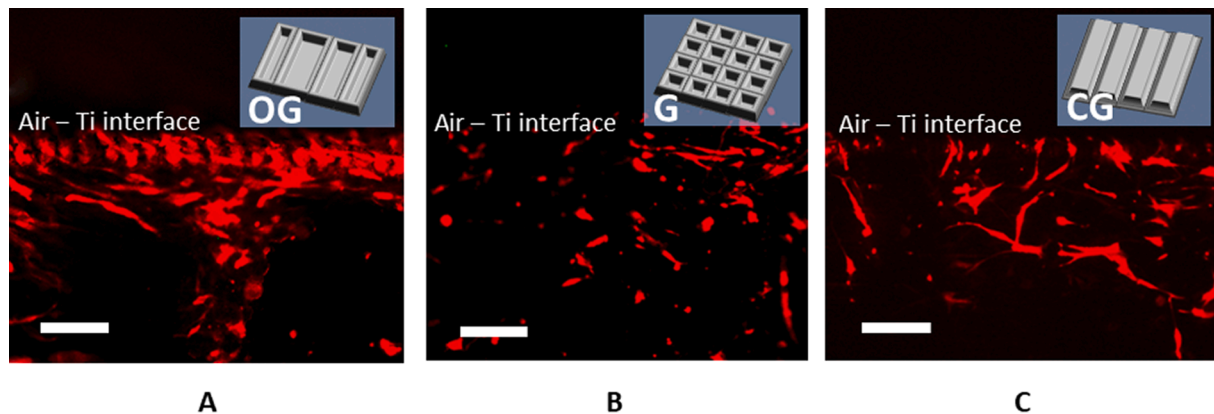


Fig. 9. Fluorescent bioimaging (on day 20th) of the seeded hMSCs Turbo FP635 into cross-sections of sample from the surface (OG (A), G (B) and CG (C) reliefs). The cells are shown by red according to the fluorescence of TurboFP635. The scale bars are  $50 \mu\text{m}$  for all images. SEM images of the cross-sections of samples before in vitro research are in Fig. 4.

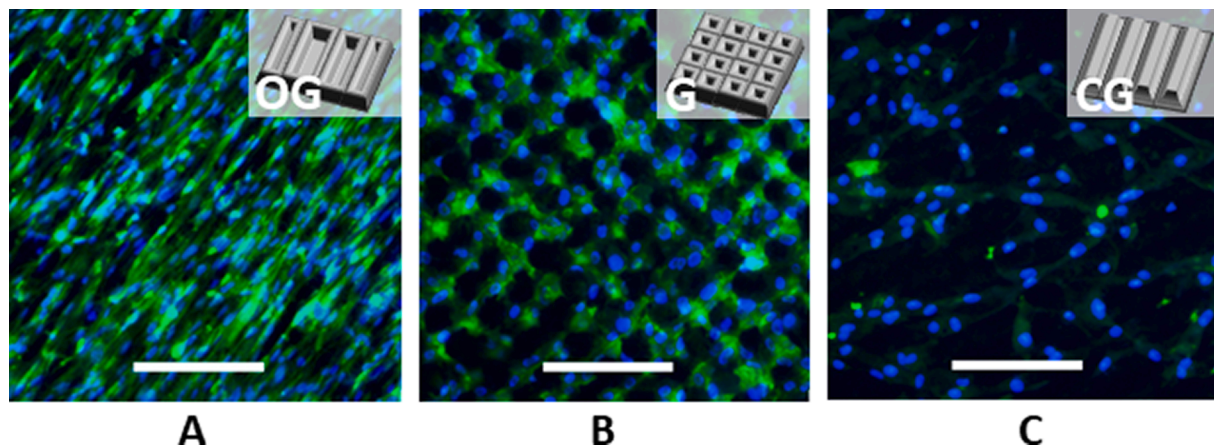


Fig. 10. Qualitative analysis of the expression of osteocalcin via immunocytochemical staining of the hMSCs with the anti-osteocalcin antibodies on day 20 on surface (OG (A), G (B) and CG (C)). Osteocalcin - green fluorescence (Opal-520); cell nuclei - blue fluorescence (Hoechst 33342). The scale bars are  $150 \mu\text{m}$  for all images.

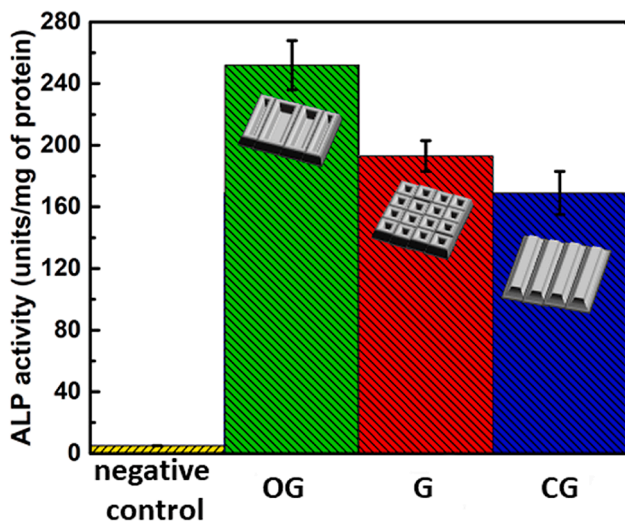


Fig. 11. Quantitative analysis of ALP activity via fluorometric assay of culture medium on day 20 for OG (B), G (C) and CG (D) reliefs.

«grid» with the period of  $49.50 (\pm 4.60) \mu\text{m}$ ,  $S_a = 11.81 (\pm 0.15) \mu\text{m}$  and  $S_{dr} = 272.00 (\pm 22.30) \%$ ; and «close grooves», with the period of  $31.40 (\pm 3.30) \mu\text{m}$ ,  $S_a = 3.26 (\pm 0.01) \mu\text{m}$  and  $S_{dr} = 43.08 (\pm 2.30) \%$ . The porous oxide layer coats the surface of the reliefs. The surface composition has a sandwich structure:  $\text{Ti} \rightarrow \text{TiO} \rightarrow \text{Ti}_2\text{O}_3\text{Nx} \rightarrow \text{TiO}_2$  (anatase)  $\rightarrow \text{TiO}_2$  (rutile).

As a result of the wettability studies, it was found that all reliefs are superhydrophilic, and the area, direction and time of spreading of a liquid droplet are different for the three presented reliefs. Maximum spreading area was achieved on the «open grooves». The fluid distributed predominantly along the grooves.

Current results clearly demonstrated that OG relief is the best for cells differentiation, alignment and osteocalcin genesis among investigated reliefs.

The proliferation study showed that, compared with the untreated titanium surface, the cells proliferated perfectly in all reliefs. However, the maximum number of cells on day 20 was found on the surface of the «open grooves» 266,500 cells/sample. The results obtained showed the cells cover both tops and bottoms of the topographies, as well as grow inward in open pores.

The in vitro study revealed that the relief affects the spatial orientation of cells: hMSCs extend along the «open grooves», while the «close grooves», which have the same roughness, does not influence the spatial orientation of cells. It was noted that the shape and size of the cell nuclei for the different topographies diverge. On the «open grooves» surface, the nuclei have the smallest size and elongated ellipsoidal shape. On the surface of the «close grooves», the cell nucleus structure was rounded and larger in size compared to the «open grooves». The cell nuclei on the grid structure are round in shape of medium size.

The osteocalcin expression study showed that osteogenesis occurred on all reliefs. The most significant amount of osteocalcin was found on «open grooves». The data are confirmed by the results of the ALP activity test.

This study demonstrates that a surface relief and  $S_a$  roughness, which significantly exceeds  $2 \mu\text{m}$ , positively affects osteogenesis, as is the case with NSCs [45]. We have found that it is beneficial for cells to have not individual slots but structures like a groove, with the distance between the peaks with subcellular to cellular scales. The results of this comprehensive study show that the cells-implants interaction between cells and implant surfaces is affected not only by surface micro-roughness, as most implant manufacturers claims, but also by the relief, which includes continuous topography with the features less than  $50 \mu\text{m}$  and the presence of nanostructures. Therefore, we suggest that it

should be taken into account the geometric structure of the surface to manufacture dental implants.

This study is preliminary and examines only cells layer as a whole. It is planned to conduct a more detailed study on the behavior of single MSCs on these structures with a description of these mechanisms and the influence of surface micro-geometry on the vital activity of cells.

## Funding

The study was supported by the Russian Science Foundation (project № 20-62-46045).

## CRediT authorship contribution statement

**Vadim Veiko:** Conceptualization, Methodology. **Yulia Karlagina:** Validation, Formal analysis, Investigation, Writing - original draft, Writing - review & editing, Visualization. **Tatiana Itina:** Writing - original draft, Writing - review & editing. **Daria Kuznetsova:** Investigation. **Vadim Elagin:** Investigation. **Elena Zagaynova:** Investigation. **Gennady Chernenko:** Resources. **Elena Egorova:** Formal analysis, Software, Writing - review & editing, Visualization. **Catherine Zernitskaia:** Conceptualization. **Sergey Manokhin:** Investigation, Writing - original draft. **Anastasia Tokmacheva-Kolobova:** Investigation. **Galina Odintsova:** Methodology, Writing - original draft, Writing - review & editing, Supervision, Project administration.

## Declaration of Competing Interest

The authors declare that they have no known competing financial interests or personal relationships that could have appeared to influence the work reported in this paper.

## Acknowledgments

The creating of thin foils using ion beams took place at the Federal Research Center «Crystallography and photonics» of Russian Academy of Science.

T. E. I. gratefully acknowledges the ITMO Invited Professorship.

G.V.O. gratefully acknowledges Eduard Ageev for fruitful discussion.

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